Wavelet Based Multigrid Reconstruction Algorithm for Optical Tomography

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A perturbation approach has been previously presented for the inverse problem in optical tomography [3]. To solve the linear perturbation equation, several iterative algorithms have been
developed, including projection onto convex sets (POCS), CGD, multigrid reconstruction [1], layer
stripping [2],[5] (for TR data), Regularized least squares (RLS) [5] [4], and total least squares
(TLS) [6]. One challenging problem in solving the perturbation equation is that the computation
complexity is usually very high due to the extremely large dimension of the weight matrix. In
order to reduce the computation time, in this paper, we propose a wavelet based multiresolution
reconstruction algorithm for solving the perturbation equation.

Let the perturbation equation be represented by $\mathbf{y} = \mathbf{H}\mathbf{x}$ and let the transform matrices for \mathbf{x} and \mathbf{y} be represented by $\mathbf{W}_{\mathbf{x}}$ and $\mathbf{W}_{\mathbf{y}}$, respectively, multiplying $\mathbf{y} = \mathbf{H}\mathbf{x}$ from left by $\mathbf{W}_{\mathbf{y}}$ and inserting $\mathbf{W}_{\mathbf{x}}^T \mathbf{W}_{\mathbf{x}} = \mathbf{I}$ in between \mathbf{H} and \mathbf{x} , we obtain:

$$\widetilde{\mathbf{H}}\ \widetilde{\mathbf{x}} = \widetilde{\mathbf{y}},\tag{1}$$

where $\tilde{\mathbf{H}} = \mathbf{W_y} \mathbf{H} \mathbf{W_x}^T$, $\tilde{\mathbf{y}} = \mathbf{W_y} \mathbf{y}$ and $\tilde{\mathbf{x}} = \mathbf{W_x} \mathbf{x}$. Here we assume the transform matrix is orthogonal so that $\mathbf{W_y}^T \mathbf{W_y} = \mathbf{I}$. Eq. (1) is the perturbation equation in the wavelet domain. By exploiting the multiresolution property of wavelet transform, multigrid method is used to reduce the computational time. Specifically, in a two grid implementation, let $\tilde{\mathbf{x}} = [\tilde{\mathbf{x}}_l, \tilde{\mathbf{x}}_h]^T$, $\tilde{\mathbf{y}} = [\tilde{\mathbf{y}}_l, \tilde{\mathbf{y}}_h]^T$, and

$$\widetilde{\mathbf{H}} = \left[\begin{array}{cc} \widetilde{\mathbf{H}}_{ll} & \widetilde{\mathbf{H}}_{lh} \\ \widetilde{\mathbf{H}}_{hl} & \widetilde{\mathbf{H}}_{hh} \end{array} \right],$$

where the subscript l represents low frequency, subscript h represents high frequency, and subscripts ll, lh, hl and hh represent LL, LH, HL and HH frequency band in wavelet decomposition, respectively. We first obtain the course grid solution by solving

$$\widetilde{\mathbf{H}}_l \ \widetilde{\mathbf{x}}_l = \widetilde{\mathbf{y}}_l \ . \tag{2}$$

This solution can be obtained very fast since the dimension of the system is reduced by half. Starting from this coarse resolution, we can obtain the full resolution solution by solving the original equation (1). Alternatively, one could choose to solve the full resolution solution for a region of interests (ROI) identified from the coarse solution.

To solve the equation in a given grid $\mathbf{\tilde{x}}_l = \mathbf{\tilde{y}}_l$, we have investigated two approaches: the regularized least squares (RLS) and the total least squares (TLS). The RLS solution is obtained by minimizing the following error formulation:

$$E(\tilde{\mathbf{x}}_l) = \|\tilde{\mathbf{H}}_l \tilde{\mathbf{x}}_l - \tilde{\mathbf{y}}_l\|^2 + \lambda_l \|\tilde{\mathbf{x}}_l\|^2, \tag{3}$$

where λ_l is a regularization parameter at the coarse resolution.

The TLS solution is obtained by solving the Rayleigh quotient equation given by:

$$Minimize F(\tilde{\mathbf{q}}_l) = \frac{\tilde{\mathbf{q}}_l^T \tilde{\mathbf{A}}_l^T \tilde{\mathbf{A}}_l \tilde{\mathbf{q}}_l}{\tilde{\mathbf{q}}_l^T \tilde{\mathbf{q}}_l}, \tag{4}$$

where

$$\widetilde{\mathbf{A}}_l = [\widetilde{\mathbf{H}}_l | \widetilde{\mathbf{y}}_l] \tag{5}$$

and

$$\widetilde{\mathbf{q}}_l = \begin{pmatrix} \widetilde{\mathbf{x}}_l \\ -1 \end{pmatrix}.$$

In the first case, the minimization is accomplished by conjugate gradient descent (CGD) method while in the second case, it is implemented by conjugate gradient (CG) method[6].

Simulation results using the RLS method in a two grid wavelet representation are shown in Fig.1.

References

- [1] Y. Wang, J. Chang, R. Aronson, R.L. Barbour, H.L. Graber, and J. Lubowsky, "Imaging scattering media by diffusion tomography: An iterative perturbation approach," in *Proc. Physiological Monitoring and Early Detection Diagnostic Methods*, vol. SPIE-1641, (Los Angeles), pp. 58-71, Jan. 1992.
- [2] J. Chang, Y. Wang, R. Aronson, H. L. Graber, and R.L. Barbour, "A layer-stripping approach for recovery of scattering media from time-resolved data," in *Proc. Inverse Problems in Scattering and Imaging*, vol. SPIE-1767, (San Diego), pp. 384-395, July 1992.
- [3] R. L. Barbour, H. L. Graber, Y. Wang, J. Chang, and R. Aronson, "A perturbation approach for optical diffusion tomography using continuous-wave and time-resolved data," SPIE Medical Optical Tomography — Functional Imaging and Monitoring, SPIE Institutes, IS11, pp. 87-120, 1993.
- [4] Y. Q. Yao, Y. Wang, Y. L. Pei, W. W. Zhu, J. H. Hu and R. L. Barb our, "Frequency Domain Optical Tomography In Human Tissue," in this proceedings.
- [5] W. Zhu, Y. Wang, H. L. Graber, R. L. Barbour and J. Chang, "A Regularized Progressive Expansion Algorithm for Recovery of Scattering Media from Time-Resolved Data," in Advances in Optical Imaging and Photon Migration, pp.211-216, edited by Robert R. Alfano, Optical Society of America, 1994.
- [6] W. Zhu, Y. Wang, J. Chang, H. L. Graber, and R. Barbour, "A Total Least Squares approach for the solution of the perturbation equation," in Proc. of Optical Tomography, Photon Migration, and Spectroscopy of Tissue and Model Media, part of An International Symposium on Biomedical optics, pp.420-430, SPIE vol. 2389, San Jose, Feb. 1995.

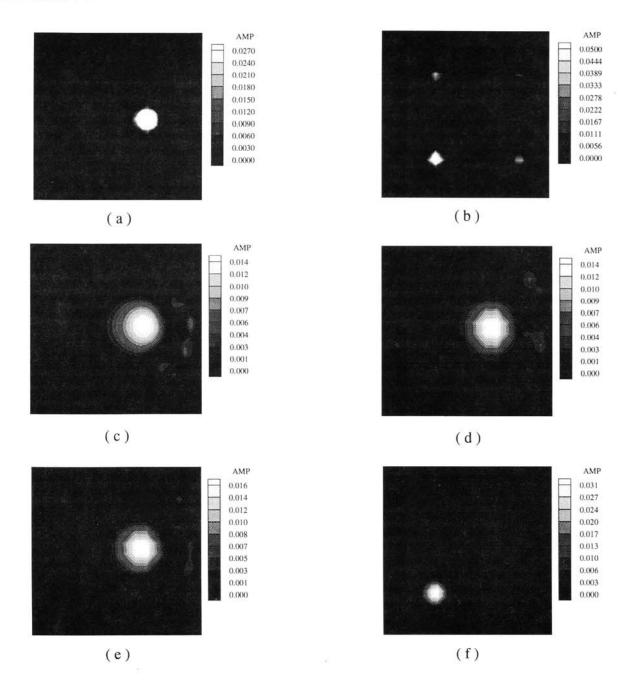


Figure 1: Reconstruction results and wavelet analysis of a medium with an off-center rod with Sin-like distribution. (a) is the original image; (b) shows the wavelet transform of original image in (a); (c) is the reconstruction result using one grid with 235 iterations; (d) is the reconstruction image using two-grids algorithm with 500 iterations in the coarse grid; (e) is the reconstruction image using two-grid algorithm with additional 200 iterations in the fine grid; and (f) is the wavelet transform of (e). The total computation time for (e) and (c) are roughly the same. The time for (d) is about 1/7 of (c).