# Simultaneous Low-Pass Filtering and Total Variation Denoising

Ivan W. Selesnick, Senior Member, IEEE, Harry L. Graber, Member, IEEE, Douglas S. Pfeil, and Randall L. Barbour

Abstract—This paper seeks to combine linear time-invariant (LTI) filtering and sparsity-based denoising in a principled way in order to effectively filter (denoise) a wider class of signals. LTI filtering is most suitable for signals restricted to a known frequency band, while sparsity-based denoising is suitable for signals admitting a sparse representation with respect to a known transform. However, some signals cannot be accurately categorized as either band-limited or sparse. This paper addresses the problem of filtering noisy data for the particular case where the underlying signal comprises a low-frequency component and a sparse or sparse-derivative component. A convex optimization approach is presented and two algorithms derived: one based on majorization-minimization (MM), and the other based on the alternating direction method of multipliers (ADMM). It is shown that a particular choice of discrete-time filter, namely zero-phase noncausal recursive filters for finite-length data formulated in terms of banded matrices, makes the algorithms effective and computationally efficient. The efficiency stems from the use of fast algorithms for solving banded systems of linear equations. The method is illustrated using data from a physiological-measurement technique (i.e., near infrared spectroscopic time series imaging) that in many cases yields data that is well-approximated as the sum of low-frequency, sparse or sparse-derivative, and noise components.

*Index Terms*—Total variation denoising, sparse signal, sparsity, low-pass filter, Butterworth filter, zero-phase filter.

## I. INTRODUCTION

INEAR TIME-INVARIANT (LTI) filters are widely used in science, engineering, and general time series analysis. The properties of LTI filters are well understood, and many effective methods exist for their design and efficient implementation [62]. Roughly, LTI filters are most suitable when the signal of interest is (approximately) restricted to a known frequency band. At the same time, the effectiveness of an alternate approach to signal filtering, based on sparsity, has been increasingly recognized [22], [34], [60], [74]. Over the past 10–15 years, the development of algorithms and theory for sparsity-

I. W. Selesnick is with the Department of Electrical and Computer Engineering, NYU Polytechnic School of Engineering, Brooklyn, NY 11201 USA (e-mail: selesi@poly.edu).

H. L. Graber, D. S. Pfeil, and R. L. Barbour are with the Department of Pathology, SUNY Downstate Medical Center, Brooklyn, NY 11203 USA.

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based signal processing has been an active research area, and many algorithms for sparsity-based denoising (and reconstruction, etc.) have been developed [67], [73]. These are most suitable when the signal of interest either is itself sparse or admits a sparse representation.

However, the signals arising in some applications are more complex: they are neither isolated to a specific frequency band nor do they admit a highly sparse representation. For such signals, neither LTI filtering nor sparsity-based denoising is appropriate by itself. Can conventional LTI filtering and more recent sparsity-based denoising methods be combined in a principled way, to effectively filter (denoise) a wider class of signals than either approach can alone?

This paper addresses the problem of filtering noisy data where the underlying signal comprises a low-frequency component and a sparse or sparse-derivative component. It is assumed here that the noisy data y(n) can be modeled as

$$y(n) = f(n) + x(n) + w(n), \quad n = 0, \dots, N - 1$$
 (1)

where f is a low-pass signal, x is a sparse and/or sparse-derivative signal, and w is stationary white Gaussian noise. For noisy data such as y in (1), neither conventional low-pass filtering nor sparsity-based denoising is suitable. Further, (1) is a good model for many types of signals that arise in practice, for example, in nano-particle biosensing (e.g., Fig. 3(a) in [30]) and near infrared spectroscopic (NIRS) imaging (e.g., Fig. 9 in [3]).

Note that if the low-pass signal f were observed in noise alone (y = f + w), then low-pass filtering (LPF) would provide a good estimate of f; i.e.,  $f \approx \text{LPF}(f + w)$ . On the other hand, if x were a sparse-derivative signal observed in noise alone (y = x + w), then total variation denoising (TVD) would provide a good estimate of x; i.e.,  $x \approx \text{TVD}(x+w)$  [68]. Given noisy data of the form y = f + x + w, we seek a simple optimization-based approach that enables the estimation of f and xindividually.

In this paper, an optimization approach is presented that enables the simultaneous use of low-pass filtering and sparsitybased denoising to estimate a low-pass signal and a sparse signal from a single noisy additive mixture, cf. (1). The optimization problem we formulate involves the minimization of a non-differentiable, strictly convex cost function. We present two iterative algorithms.<sup>1</sup> The first algorithm models x in (1) as having a sparse derivative and is derived using the majorization-minimization (MM) principle. The second algorithm models x in (1) as having a sparse derivative, or being sparse itself, or both. This algorithm is derived using the alternating direction method of multipliers (ADMM). The second algorithm is more general

<sup>1</sup>Software is available at http://eeweb.poly.edu/iselesni/lpftvd/

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and can be used in place of the first. However, as will be illustrated below (Section VII-C), in cases where the first algorithm is applicable, it is preferable to the second one, because it converges faster and does not require a step-size parameter as the second algorithm does.

In addition, this paper explains how a suitable choice of discrete-time filter makes the proposed approach effective and computationally efficient. Namely, we describe the design and implementation of a zero-phase non-causal recursive filter for finite-length data, formulated in terms of banded matrices. We choose recursive filters for their computational efficiency in comparison with non-recursive filters, and the zero-phase property to eliminate phase distortion (phase/time offset issues). As the algorithms are intended primarily for batch-mode processing, the filters need not be causal. We cast the recursive discrete-time filter in terms of a matrix formulation so as to easily and accurately incorporate it into the optimization framework and because it facilitates the implementation of the filter on finite-length data. Furthermore, the formulation is such that all matrix operations in the devised algorithms involve only banded matrices, thereby exploiting the high computational efficiency of solvers for banded linear systems ([65], Section 2.4) and of sparse matrix multiplication.

The computational efficiency of the proposed algorithms also draws on recent developments in sparse-derivative signal denoising (i.e., total variation (TV) denoising [10], [19], [68]). In particular, we note that the exact solution to the 1D TV denoising problem can be calculated by fast constructive algorithms [27], [49]. The algorithms presented here draw on this and the 'fused lasso signal approximator' [40].

After Section II on preliminaries, Section III presents the formulation of the optimization problem for simultaneous low-pass filtering and sparse-signal denoising. Section IV derives an iterative algorithm for solving the optimization problem. Section V addresses the case where both the signal itself and its derivative are sparse. Section VI presents recursive discrete-time filters to be used in the algorithms. Section VII illustrates the proposed algorithms on data, including NIRS times series.

## A. Related Work

The problem addressed in this paper is closely related to the problem addressed in [70], [71]; however, the new approach described here has several advantages over the method described there. While [71] uses least squares polynomial approximation on overlapping blocks for signal smoothing, the new approach uses LTI filtering. As a consequence, the new approach results in a time-invariant signal processing algorithm, in contrast to the approach of [71]. In addition, compared with [71], the new approach employs a more general sparse-derivative model that incorporates the sparsity of both the signal and its derivative. This is useful in practice for separating transient waveforms/pulses from a low-frequency background signal. Also, unlike [71], one of the new algorithms is devised so that sparse-derivative denoising is an explicit step, which means that new fast methods for TV denoising (e.g. [27]) can be readily incorporated.

The approach taken in this paper is also related to that of [44], in which Tikhonov (quadratic) and total variation regularizations are simultaneously used for the denoising and reconstruction of piecewise-smooth signals. Reference [44] also addresses general linear inverse problems, and involves both 1D signals and images. The work described in this paper can be differentiated from that of [44] by noting that this work: (1) utilizes LTI filtering, which provides a more convenient way to specify the frequency response of the smoothing operator, in comparison with Tikhonov regularization, (2) utilizes compound regularization (see Section II-C), and (3) explicitly exploits fast algorithms for banded systems.

Many papers have addressed the problem of filtering/denoising piecewise smooth signals, a class of signals that includes the signals taken up in this paper, i.e., y in (1). However, as noted in [71], much of the work on this topic explicitly or implicitly models the underlying signal of interest as being composed of smooth segments separated by discontinuities (or blurred discontinuities) [16], [33], [57]. This is particularly appropriate in image processing wherein distinct smooth regions correspond to distinct objects and discontinuities correspond to the edges of objects (e.g. one object occluding another) [43]. Under this model, smoothing across discontinuities should be avoided, to prevent blurring of edges. The signal model (1) taken up in this paper differs in an important way: it models the smooth behavior on the two sides of a discontinuity as being due to a common low-pass signal, i.e., f in (1). In contrast to most methods developed for processing piecewise smooth signals, the proposed method seeks to exploit the common smooth behavior on both sides of a discontinuity, as in [44], [70], [71].

The problem addressed in this paper is a type of sparsitybased denoising problem, and, as such, it is related to the general problem of sparse signal estimation. Many papers, especially over the last fifteen years, have addressed the problem of filtering/denoising signals, both 1D and multidimensional, using sparse representations via suitably chosen transforms (wavelet, etc.) [29], [53], [64]. The method described here has some similarities to sparse transform-domain filtering [60]. For example, in wavelet-domain thresholding, the low-pass wavelet subband is often left intact (no thresholding is applied to it). In this case, a large threshold value leads to a denoised signal that is essentially a low-pass filtered version of the noisy data. When the threshold is small, the result of wavelet-domain thresholding is essentially the noisy data itself. Likewise, the proposed algorithms involve a regularization parameter  $\lambda$ . When  $\lambda$  is set to a large value, the algorithms essentially perform low-pass filtering; when  $\lambda$  is small, the algorithms leave the data essentially unchanged.

More generally, as wavelet and related multiscale transforms [17], [55] include a low-pass subband, which can be regularized separately from other subbands, wavelet-domain processing provides the opportunity to combine low-pass filtering and sparsity-based processing in a single framework. However, the proposed approach differs from many wavelet-based approaches in several aspects. For one, it completely decouples the low-pass filter from the sparse-signal description, while in wavelet-domain denoising the low-pass subband/filter is determined by the specific wavelet transform utilized. Hence, in the proposed approach, the design of the low-pass filter can be based on the properties of the low-pass component in the signal model (f in (1)). Moreover, the proposed method, not being based on transform-domain sparsity, avoids the complications associated with selecting and implementing a suitable wavelet (or other) transform (choice of transform, choice of wavelet filters, boundary extensions, radix-2 length constraints, etc.). In addition, as the proposed approach is based on TV denoising, it avoids the 'pseudo-Gibbs' phenomenon that is present to varying degree in many wavelet-based methods [23].

The concept, employed in this work, of modeling a signal as the sum of two distinct components, has a history in image processing [5], [15], [75]. In particular, the problem of expressing an image as a sum of texture and geometry components has been effectively addressed by sparse representation techniques [6], [72]. These techniques are also useful in 1D signal processing [31], [69]. Following these works, the approach used in this paper utilizes the technique of sparsity-based signal separation; however, in this paper sparsity is used to model only one of the two signal components.

A cornerstone of sparsity-based signal processing is the availability of optimization algorithms that are simultaneously: robust, computationally efficient, and suitable for a broad class of non-smooth convex problems. An important class of such algorithms is based on proximity operators [25]. Recent algorithmic developments in non-smooth convex optimization make feasible the solution of a wide class of non-smooth problems [14], [20], [26], [28], [63], [66], [76]. These algorithms are especially suitable for minimizing the sum of several non-smooth functions, which is particularly relevant to this work.

#### B. Near Infrared Spectroscopy (NIRS)

The proposed algorithms are illustrated on experimental data obtained from a NIRS time-series measurement system [9], which, as indicated above, frequently produces data that are well approximated by the model in (1). The NIRS physiological modality uses light at two or more wavelengths in the  $\sim (690-1000)$  nm range to monitor spatiotemporal fluctuations in tissue blood volume and blood oxygen saturation (we refer to these collectively as the 'hemodynamic variables') [8]. For a number of reasons, it is prone to producing time-series data that are well described by the model (1):

- Not uncommonly, there are long-term drifts in hemodynamic variables within the probed tissue volume (e.g., resulting from blood-pressure fluctuations) during the course of the measurement. These produce a low-frequency component in the data.
- Additionally, the hemodynamic signal arises primarily from small blood vessels (arterioles, capillaries, venules) that tend to exhibit low-frequency oscillations called vasomotion [61].
- 3) Many NIRS measurement paradigms involve the intermittent presentation of stimuli to, or performance of tasks by, the human or animal subject [51]. These are intended to produce shifts in the magnitude of the hemodynamic variables approximately concurrent with the challenges, followed by a return to the previous level. That is, the signal is both sparse (i.e., resides at the baseline level most of the time) and has a sparse derivative (i.e., departs from the baseline a small number of times during the course of the measurement).
- However, not all measurements are intervention-based. Resting-state monitoring also can be biologically informative and is commonly performed [77].
- 5) Unplanned events (e.g., postural shift, or subject sneezes) can introduce unwanted signal components that are sparse or have a sparse derivative.

The preceding considerations indicate that, depending on the experimental-design context, either the low-frequency or the sparse component may be the biological signal of interest.

#### **II. PRELIMINARIES**

# A. Notation

Vectors and matrices are represented by lower- and uppercase bold respectively (e.g.,  $\mathbf{x}$  and  $\mathbf{H}$ ). Finite-length discretetime signals will be represented as lower-case italicized or bold. The N-point signal x is represented by the vector

$$\mathbf{x} = [x(0), \dots, x(N-1)]^T$$

where  $[\cdot]^T$  denotes the transpose. Matrix **D** is defined as

$$\mathbf{D} := \begin{bmatrix} -1 & 1 & & \\ & -1 & 1 & \\ & & \ddots & \ddots & \\ & & & -1 & 1 \end{bmatrix}.$$
 (2)

The first-order difference of an N-point signal  $\mathbf{x}$  is given by  $\mathbf{D}\mathbf{x}$ where  $\mathbf{D}$  is of size  $(N - 1) \times N$ .

The notation  $\|\mathbf{v}_1\|$ , defined as  $\|\mathbf{v}_1\| = \sum_n |v(n)|$ , denotes the  $\ell_1$  norm of the vector  $\mathbf{v}$ . The notation  $\|\mathbf{v}\|_2$ , defined as  $\|\mathbf{v}\|_2 = (\sum_n |v(n)|^2)^{1/2}$ , denotes the  $\ell_2$  norm of the vector  $\mathbf{v}$ .

The soft-threshold function [32] is defined as

$$\operatorname{soft}(x,T) := \begin{cases} x - T(x/|x|), & |x| > T\\ 0 & |x| \leqslant T \end{cases}$$

for  $x \in \mathbb{C}$  and T > 0. This is the usual soft-threshold function on the real line, generalized here to the complex plane. For a vector  $\mathbf{x}$  or signal x(n), the notation  $\operatorname{soft}(\mathbf{x}, T)$  refers to the soft-threshold function applied element-wise to  $\mathbf{x}$ .

## B. Total Variation Denoising

Sparse-derivative signal denoising refers to the problem of estimating a signal x, having a sparse or approximately sparse derivative, from a noisy observation, e.g. y = x + w. As is well known, the  $\ell_1$  norm is a convex proxy for sparsity, so it is practical to formulate sparse-derivative denoising as the problem of minimizing the  $\ell_1$  norm of the derivative of x subject to a data fidelity constraint. For discrete-time data, the simplest approximation of the derivative is the first-order difference; hence, consider the minimization of  $\|\mathbf{Dx}\|_1$ . Assuming the N-point signal  $\mathbf{x}$  is observed in additive white Gaussian noise with variance  $\sigma^2$ , a suitable data fidelity constraint is  $\|\mathbf{y} - \mathbf{x}\|_2^2 \leq N\sigma^2$ . This leads to the constrained optimization problem

$$\underset{\mathbf{x}}{\operatorname{argmin}} \quad \|\mathbf{D}\mathbf{x}\|_1 \tag{3a}$$

such that 
$$\|\mathbf{y} - \mathbf{x}\|_2^2 \leq N \sigma^2$$
. (3b)

Problem (3) is equivalent, for suitable  $\lambda$ , to the unconstrained optimization problem

$$\arg\min_{\mathbf{x}} \left\{ \frac{1}{2} \|\mathbf{y} - \mathbf{x}\|_{2}^{2} + \lambda \|\mathbf{D}\mathbf{x}\|_{1} \right\},$$
(4)

i.e.,

$$\arg \min_{x} \frac{1}{2} \sum_{n=0}^{N-1} |y(n) - x(n)|^2 + \lambda \sum_{n=1}^{N-1} |x(n) - x(n-1)|.$$

Problems (3) and (4) are two forms of the *total variation denoising* (TVD) problem [21]. The unconstrained form (4) is more commonly used than the constrained form (3).

We will denote the solution to problem (4) as  $tvd(\mathbf{y}, \lambda)$ ,

$$\operatorname{tvd}(\mathbf{y},\,\lambda) := \arg\,\min_{\mathbf{x}} \left\{ \frac{1}{2} \|\mathbf{y} - \mathbf{x}\|_{2}^{2} + \lambda \|\mathbf{D}\mathbf{x}\|_{1} \right\}.$$
(5)

There is no explicit solution to (4), but a fast algorithm to compute the exact solution has been developed [27] (with a C implementation).

Increasing the parameter  $\lambda$  has the effect of making the solution **x** more nearly piecewise constant. Instead of the first-order difference, other approximations of derivatives can be used for sparse-derivative denoising. The notion of total variation has been further generalized in several ways to make it effective for a broader class of signals [13], [52], [56], [59].

# C. Fused Lasso Signal Approximator

If both the signal  $\mathbf{x}$  and its derivative are sparse, then the denoising problem is more appropriately formulated as

$$\arg\min_{\mathbf{x}} \left\{ \frac{1}{2} \|\mathbf{y} - \mathbf{x}\|_{2}^{2} + \lambda_{0} \|\mathbf{x}\|_{1} + \lambda_{1} \|\mathbf{D}\mathbf{x}\|_{1} \right\}.$$
(6)

This is a special case of a compound penalty function [1], [11], wherein two or more regularizers are used to promote distinct properties of the signal to be recovered.

The specific problem (6) is referred to as the 'fused lasso signal approximator' in [40]. Interestingly, Proposition 1 in [40] shows that problem (6) is equivalent to (4) in the sense that the solution to (6) can be obtained explicitly from the solution to (4). Specifically, the solution to (6) is given by

$$\mathbf{x} = \text{soft}(\text{tvd}(\mathbf{y}, \lambda_1), \lambda_0). \tag{7}$$

Hence, it is not necessary to have a separate algorithm for (6); it suffices to have an algorithm for the TVD problem (5).

# D. Majorization-Minimization

The MM procedure replaces a difficult minimization problem with a sequence of simpler ones [38]. To minimize a function  $F(\mathbf{x})$ , the MM procedure produces a sequence  $\mathbf{x}_k$  according to

$$\mathbf{x}_{k+1} = \arg\min_{\mathbf{x}} G_k(\mathbf{x}) \tag{8}$$

where k is the iteration index,  $k \ge 0$ . The function  $G_k(\mathbf{x})$  is any convex majorizer of  $F(\mathbf{x})$  (i.e.,  $G_k(\mathbf{x}) \ge F(\mathbf{x}) \forall \mathbf{x}$ ) that coincides with  $F(\mathbf{x})$  at  $\mathbf{x}_k$  (i.e.,  $G_k(\mathbf{x}_k) = F(\mathbf{x}_k)$ ). With initialization  $\mathbf{x}_0$ , the update (8) produces a sequence  $\mathbf{x}_k$  converging to the minimizer of  $F(\mathbf{x})$ . For more details, see [38] and references therein.

Below, a majorizer for the  $\ell_1$  norm will be used. To that end, note that

$$\frac{1}{2}\mathbf{x}^{T}\boldsymbol{\Lambda}_{k}^{-1}\mathbf{x} + \frac{1}{2}\|\mathbf{x}_{k}\|_{1} \ge \|\mathbf{x}\|_{1}, \quad \boldsymbol{\Lambda}_{k} = \operatorname{diag}(|\mathbf{x}_{k}|), \quad (9)$$

with equality when  $\mathbf{x} = \mathbf{x}_k$ . Therefore, the left-hand-side of (9) is a majorizer of  $||\mathbf{x}||_1$  and we will use it as  $G(\mathbf{x})$  in the MM procedure. Equation (9) is a direct consequence of  $(|x| - |x_k|)^2 \ge 0$  for  $x, x_k \in \mathbb{R}$ .

# **III. PROBLEM FORMULATION**

Consider the problem of observing a noisy additive mixture of a low-pass signal f and a sparse-derivative signal x,

$$y = f + x + w, \tag{10}$$

where it is assumed that w is stationary white Gaussian noise with variance  $\sigma^2$ . We seek estimates

$$\hat{x} \approx x, \quad \hat{f} \approx f.$$
 (11)

Given an estimate  $\hat{x}$  of x, we will estimate f as

$$\hat{f} := \mathsf{LPF}(y - \hat{x}),\tag{12}$$

where LPF is a specified low-pass filter. Therefore, the problem is to find  $\hat{x}$ .

Using (12) in (11), we should choose  $\hat{x}$  so that

$$\mathsf{LPF}(y - \hat{x}) \approx f. \tag{13}$$

Using (10) in (13) gives

$$\mathsf{LPF}(y - \hat{x}) \approx y - x - w. \tag{14}$$

Using (11) in (14) gives

$$\mathsf{LPF}(y - \hat{x}) \approx y - \hat{x} - w \tag{15}$$

or

$$(y - \hat{x}) - \mathsf{LPF}(y - \hat{x}) \approx w.$$
(16)

Note that the left-hand side of (16) constitutes a high-pass filter of  $y - \hat{x}$ . (This assumes that the frequency response of the low-pass filter is zero-phase or at least approximately zero-phase.)

Defining HPF := I - LPF, we write (16) as

$$\mathsf{HPF}(y - \hat{x}) \approx w. \tag{17}$$

The expression (16) contains the data y, the estimate  $\hat{x}$  that we seek to determine, and the noise signal w, but not the unknown signal f or x; hence, it can be used to derive an estimate  $\hat{x}$ . Using bold-face **H** to represent the high-pass filter matrix, we have  $\mathbf{H}(\mathbf{y} - \hat{\mathbf{x}}) \approx \mathbf{w}$ .

Hence,  $\hat{\mathbf{x}}$  should be chosen so that  $\mathbf{H}(\mathbf{y} - \hat{\mathbf{x}})$  resembles a white Gaussian random vector with variance  $\sigma^2$ . At the same time,  $\hat{\mathbf{x}}$  should have a sparse derivative; i.e., the  $\ell_1$  norm of  $\mathbf{D}\mathbf{x}$  should be small. Therefore, the estimation of  $\mathbf{x}$  can be formulated as the constrained optimization problem

$$\arg\min_{\mathbf{x}} \|\mathbf{D}\mathbf{x}\|_1 \tag{18a}$$

such that 
$$\|\mathbf{H}(\mathbf{y} - \mathbf{x})\|_2^2 \leq N \sigma^2$$
. (18b)

For suitable  $\lambda$ , an equivalent formulation is the unconstrained optimization problem:

$$\arg\min_{\mathbf{x}} \left\{ \frac{1}{2} \|\mathbf{H}(\mathbf{y} - \mathbf{x})\|_{2}^{2} + \lambda \|\mathbf{D}\mathbf{x}\|_{1} \right\}.$$
 (19)

We refer to (18) and (19) as the LPF/TVD problem, the unconstrained form being computationally easier to solve. In Section IV, we derive an algorithm for solving (19), and consider the selection of a suitable  $\lambda$ .

We will set the high-pass filter H to be of the form

$$\mathbf{H} = \mathbf{A}^{-1}\mathbf{B},\tag{20}$$

where **A** and **B** are banded matrices. The design of the filter **H** is presented in Section VI, where it will be seen that the mathematical form of (20) flows naturally from the standard difference-equation formulation of LTI filtering. Note that while **A** is banded,  $\mathbf{A}^{-1}$  is not, and hence neither is **H**.

The low-pass filter LPF to estimate f in (12) will be given by LPF = I - HPF with filter matrix  $L = I - A^{-1}B$ .

#### IV. LPF/TVD ALGORITHM

Large-scale non-differentiable convex optimizations arise in many signal/image processing tasks (sparsity-based denoising, deconvolution, compressed sensing, etc.). Consequently, numerous effective algorithms have been developed for such problems, particularly for those of the form (19) [24], [35], [46]. In this section we apply the 'majorization-minimization' (MM) approach [38] to develop an algorithm for solving (19).

Note that the solution to (19) is unique only up to an additive constant. To make the solution unique, and to facilitate the subsequent use of MM, the following change of variables can be used. Let

$$\mathbf{x} = \mathbf{S}\mathbf{u} \tag{21}$$

where  $\mathbf{S}$  is a matrix of the form

$$\mathbf{S} := \begin{bmatrix} 0 & & & & \\ 1 & 0 & & & \\ 1 & 1 & 0 & & \\ \vdots & & \ddots & \\ 1 & 1 & \cdots & 1 & 0 \\ 1 & 1 & \cdots & 1 & 1 \end{bmatrix}$$
(22)

of size  $N \times (N - 1)$ . It represents a cumulative sum. Note that

$$\mathbf{DS} = \mathbf{I},\tag{23}$$

i.e., S is a discrete anti-derivative. Therefore,

$$\mathbf{D}\mathbf{x} = \mathbf{D}\mathbf{S}\mathbf{u} = \mathbf{u}.$$
 (24)

We also note that for the filters to be introduced in Section VI, the matrix  $\mathbf{B}$  can be expressed as

$$\mathbf{B} = \mathbf{B}_1 \mathbf{D} \tag{25}$$

where  $\mathbf{B}_1$  is banded matrix. This factorization is used in the algorithm derivation below. The fact that  $\mathbf{B}_1$  is banded is also important for the computational efficiency of the algorithm.

With (21), problem (19) can be written as

$$\arg\min_{\mathbf{u}} \left\{ F(\mathbf{u}) = \frac{1}{2} \|\mathbf{H}(\mathbf{y} - \mathbf{S}\mathbf{u})\|_2^2 + \lambda \|\mathbf{u}\|_1 \right\}.$$
 (26)

With the optimal solution  $\mathbf{u}$ , the solution to (19) is obtained as  $\mathbf{x} = \mathbf{S}\mathbf{u}$ . To minimize (26) using MM, we need a majorizer  $G_k(\mathbf{u})$  of the cost function  $F(\mathbf{u})$  in (26). Using (9), a majorizer of  $F(\mathbf{u})$  is given by

$$G_k(\mathbf{u}) = \frac{1}{2} \|\mathbf{H}(\mathbf{y} - \mathbf{S}\mathbf{u})\|_2^2 + \frac{\lambda}{2} \mathbf{u}^T \mathbf{\Lambda}_k^{-1} \mathbf{u} + \frac{\lambda}{2} \|\mathbf{u}_k\|_1,$$

where  $\Lambda_k$  is the diagonal matrix,

$$[\mathbf{\Lambda}_k]_{n,n} = |\mathbf{u}_k(n)|.$$

Using (20), (23) and (25),

$$\mathbf{HS} = \mathbf{A}^{-1}\mathbf{BS} = \mathbf{A}^{-1}\mathbf{B}_{1}\mathbf{DS} = \mathbf{A}^{-1}\mathbf{B}_{1},$$

and the majorizer can be written as

$$G_k(\mathbf{u}) = \frac{1}{2} \|\mathbf{A}^{-1}\mathbf{B}\mathbf{y} - \mathbf{A}^{-1}\mathbf{B}_1\mathbf{u}\|_2^2 + \frac{\lambda}{2}\mathbf{u}^T\mathbf{\Lambda}_k^{-1}\mathbf{u} + C$$

where C does not depend on u. The MM update is given by

$$\mathbf{u}_{k+1} = \arg\min_{\mathbf{u}} G_k(\mathbf{u}) \tag{27}$$

which has the explicit form

$$\mathbf{u}_{k+1} = \left(\mathbf{B}_1^T (\mathbf{A}\mathbf{A}^T)^{-1} \mathbf{B}_1 + \lambda \mathbf{\Lambda}_k^{-1}\right)^{-1} \mathbf{B}_1^T (\mathbf{A}\mathbf{A}^T)^{-1} \mathbf{B}\mathbf{y}.$$

A numerical problem is that as the iterations progress, many values of  $\mathbf{u}_k$  are expected to go to zero (due the sparsity promoting properties of the  $\ell_1$  norm), and therefore some entries of  $\mathbf{\Lambda}_k^{-1}$  will go to infinity. This issue is addressed, as described in [39], by rewriting the equation using the matrix inverse lemma:

$$\left( \mathbf{B}_{1}^{T} (\mathbf{A}\mathbf{A}^{T})^{-1} \mathbf{B}_{1} + \lambda \mathbf{\Lambda}_{k}^{-1} \right)^{-1}$$

$$= \frac{1}{\lambda} \mathbf{\Lambda}_{k} - \frac{1}{\lambda} \mathbf{\Lambda}_{k} \mathbf{B}_{1}^{T} \left( \underbrace{\lambda \mathbf{A}\mathbf{A}^{T} + \mathbf{B}_{1} \mathbf{\Lambda}_{k} \mathbf{B}_{1}^{T}}_{\text{banded}} \right)^{-1} \mathbf{B}_{1} \mathbf{\Lambda}_{k}.$$
 (28)

The indicated matrix is banded because A,  $B_1$ , and  $\Lambda_k$  are all banded. Using (28), the MM update (27) can be implemented as:

$$\begin{aligned} \mathbf{b} &\leftarrow \frac{1}{\lambda} \mathbf{B}_1^T (\mathbf{A} \mathbf{A}^T)^{-1} \mathbf{B} \mathbf{y} \\ \mathbf{\Lambda}_k &\leftarrow \operatorname{diag}(|\mathbf{u}_k|) \\ \mathbf{u}_{k+1} &\leftarrow \mathbf{\Lambda}_k \left[ \mathbf{b} - \mathbf{B}_1^T \left( \lambda \mathbf{A} \mathbf{A}^T + \mathbf{B}_1 \mathbf{\Lambda}_k \mathbf{B}_1^T \right)^{-1} \mathbf{B}_1 \mathbf{\Lambda}_k \mathbf{b} \right]. \end{aligned}$$

The update can be implemented using fast solvers for banded systems of linear equations [14], [47] ([65], Section 2.4). Furthermore, as all matrices are banded, matrix-vector multiplications are also computationally efficient.

The update equations constitute an algorithm, Algorithm 1, solving the LPF/TVD problem (19). Once x is computed, the low-pass component,  $\mathbf{f}$ , is obtained by applying the low-pass filter  $\mathbf{L} = \mathbf{I} - \mathbf{A}^{-1}\mathbf{B}$  to  $(\mathbf{y} - \mathbf{x})$ , cf. (12).

Algorithm 1	1: For t	e LPF/TVD	problem (	(19)
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Input:  $\mathbf{y} \in \mathbb{R}^N$ ,  $\lambda > 0$ Output:  $\mathbf{x}, \mathbf{f} \in \mathbb{R}^N$ 1:  $\mathbf{b} \leftarrow (1/\lambda) \mathbf{B}_1^T (\mathbf{A}\mathbf{A}^T)^{-1} \mathbf{B}\mathbf{y}$ 2:  $\mathbf{u} \leftarrow \mathbf{D}\mathbf{y}$ 3: repeat 4:  $\mathbf{\Lambda} \leftarrow \operatorname{diag}(|\mathbf{u}|)$ 5:  $\mathbf{Q} \leftarrow \lambda \mathbf{A}\mathbf{A}^T + \mathbf{B}_1\mathbf{\Lambda}\mathbf{B}_1^T$ 6:  $\mathbf{u} \leftarrow \mathbf{\Lambda}[\mathbf{b} - \mathbf{B}_1^T\mathbf{Q}^{-1}\mathbf{B}_1\mathbf{\Lambda}\mathbf{b}]$ 7: until convergence 8:  $\mathbf{x} \leftarrow \mathbf{S}\mathbf{u}$ 9:  $\mathbf{f} \leftarrow (\mathbf{y} - \mathbf{x}) - \mathbf{A}^{-1}\mathbf{B}(\mathbf{y} - \mathbf{x})$ 10: return  $\mathbf{x}, \mathbf{f}$ 

The change of variables  $\mathbf{x} = \mathbf{Su}$  is important above, because otherwise the MM approach leads here to a dense system of equations. The efficiency of the algorithm relies on the system being banded. Each iteration has O(dN) computational cost, where d is the order of the filter **H**. Our implementation is programmed in MATLAB which in turn uses LAPACK for solving banded systems [4], [45].

*Optimality Conditions:* The optimality conditions characterizing the minimizer of (19) can be adapted from [41] and Prop 1.3 of [7]. Define

$$\mathbf{g} = \mathbf{S}^T \mathbf{H}^T \mathbf{H} (\mathbf{y} - \mathbf{x}), \quad \mathbf{u} = \mathbf{D} \mathbf{x}.$$
 (29)

Then x minimizes (19) if and only if

$$g(n) = \operatorname{sign}(u(n)) \cdot \lambda, \quad \text{for } u(n) \neq 0$$
  

$$|g(n)| \leq \lambda, \quad \text{for } u(n) = 0.$$
(30)

Using (30), one can readily verify the optimality of a result produced by a numerical algorithm.

Setting  $\lambda$ : The optimality condition (30) can be used as a guideline to set the regularization parameter  $\lambda$ . We follow an approach like that described in Section 4.1 of [42]. Note that if **y** consists of noise only (i.e.,  $\mathbf{y} = \mathbf{w}$ ), then (ideally) **x** will be identically zero. From (29), **g** and **u** are given in this case by  $\mathbf{g} = \mathbf{S}^T \mathbf{H}^T \mathbf{H} \mathbf{w}$  and  $\mathbf{u} = \mathbf{0}$ . This is optimal, according to (30), if  $\lambda \ge \max(\mathbf{g}) = \max(\mathbf{S}^T \mathbf{H}^T \mathbf{H} \mathbf{w})$ . Choosing the minimal  $\lambda$ , in order to avoid unnecessary attenuation/distortion of **x**, we get the value

$$\lambda = \max(\mathbf{S}^T \mathbf{H}^T \mathbf{H} \mathbf{w}) \tag{31}$$

which assumes availability of the noise signal w. Start- and end-transients should be omitted when using (31). In practice, the noise is not known, but its statistics may be known and an approximate maximum value precomputed. For example, if the noise is zero-mean white Gaussian with variance  $\sigma^2$ , then we may compute the standard deviation of  $\mathbf{S}^T \mathbf{H}^T \mathbf{H} \mathbf{w}$  and use the 'three-sigma' rule (or similar) in place of the maximum value, to obtain the guideline  $\lambda = 3 \operatorname{std}(\mathbf{S}^T \mathbf{H}^T \mathbf{H} \mathbf{w})$ . Note that this approach for setting  $\lambda$  uses no information regarding the signal **x** or its statistics. Therefore, as a non-Bayesian procedure, it will not give a value for  $\lambda$  that is optimal in the mean-square sense. However, it can be useful in practice and can be used as a reasonable starting point for other schemes for optimizing regularization parameters.

#### V. COMPOUND SPARSE DENOISING

In this section, the signal x is modeled as being sparse itself and having a sparse derivative. As in Section III, we will estimate the low-pass component f by applying a low-pass filter to  $(y - \hat{x})$ . In order to estimate x, instead of solving (19), we solve

$$\arg\min_{\mathbf{x}} \left\{ \frac{1}{2} |\mathbf{H}(\mathbf{y} - \mathbf{x})||_{2}^{2} + \lambda_{0} ||\mathbf{x}||_{1} + \lambda_{1} ||\mathbf{D}\mathbf{x}||_{1} \right\}$$
(32)

which promotes sparsity of both x and its first-order difference. The high-pass filter  $\mathbf{H} = \mathbf{A}^{-1}\mathbf{B}$  is the same as used above, as it reflects the behavior of the low-pass component f. We refer to (32) as the LPF/CSD problem ('CSD' for compound sparse denoising).

The use of two regularizers as in (32) is referred to as compound regularization. Algorithms for compound regularization are given in [1], [11], which consider as an example, the restoration of images that are both sparse and have sparse gradients. Algorithms for more general and challenging forms of compound regularization, in which possibly all terms are non-smooth, have also been developed [6], [26], [28], [63]. The particular compound regularization in (32) was also addressed in [40], as noted in Section II-C. In the following, we use Proposition 1 of [40], i.e., (7).

If the MM process were used, as in Section IV, to develop an algorithm for solving (32), then each iteration of the resulting algorithm would require solving a dense (not-banded) system of N linear equations, where N is the length of the signal  $\mathbf{x}$ . This significantly increases the computational cost (by factor N). Therefore, in this section we apply the 'alternating direction method of multipliers' (ADMM) [2], [12]. ADMM is closely related to the split-Bregman algorithm and its variations [46], [78]. It can also be viewed as the Douglas-Rachford algorithm applied to the dual problem [25], [66].

As in [2], we apply 'variable splitting' to decouple the terms of the cost function. In this case, problem (32) can be rewritten as the constrained problem:

$$\arg\min_{\mathbf{x},\mathbf{v}}\left\{\frac{1}{2}\|\mathbf{H}\mathbf{y}-\mathbf{H}\mathbf{x}\|_{2}^{2}+\lambda_{0}\|\mathbf{v}\|_{1}+\lambda_{1}\|\mathbf{D}\mathbf{v}\|_{1}\right\} \quad (33a)$$

such that 
$$\mathbf{v} = \mathbf{x}$$
. (33b)

Applying ADMM to (33) yields the iterative algorithm:

$$\mathbf{x} \leftarrow \arg \min_{\mathbf{x}} \|\mathbf{H}\mathbf{y} - \mathbf{H}\mathbf{x}\|_{2}^{2} + \mu \|\mathbf{v} - \mathbf{x} - \mathbf{d}\|_{2}^{2}$$
(34a)

$$\mathbf{v} \leftarrow \arg\min_{\mathbf{v}} \lambda_0 \|\mathbf{v}\|_1 + \lambda_1 \|\mathbf{D}\mathbf{v}\|_1 + 0.5 \,\mu \|\mathbf{v} - \mathbf{x} - \mathbf{d}\|_2^2$$

(34b)

$$\mathbf{d} \leftarrow \mathbf{d} - (\mathbf{v} - \mathbf{x}) \tag{34c}$$

The iterative algorithm (34) alternates between minimization with respect to x in (34a) and v in (34b).

The algorithm (34) requires that the parameter  $\mu > 0$  be specified; the value of  $\mu$  does not affect the solution to which the algorithm converges, but it does affect the overall convergence behavior. The convergence may be slow for a poor value of  $\mu$ (see LPF/CSD Example 1, below). The variables d and v also must be initialized prior to the loop; however, as the cost function is convex, the algorithm converges to the unique minimizer regardless of the initialization [12]. We initialize both d and v to all-zero vectors the same size as y. The loop is repeated until some stopping criterion is satisfied.

The solution to (34a) can be expressed as

$$\mathbf{x} \leftarrow (\mathbf{H}^T \mathbf{H} + \mu \mathbf{I})^{-1} (\mathbf{H}^T \mathbf{H} \mathbf{y} + \mu (\mathbf{v} - \mathbf{d})).$$
(35)

From (20), we write

$$\mathbf{H}^T \mathbf{H} \mathbf{y} = \mathbf{B}^T (\mathbf{A} \mathbf{A}^T)^{-1} \mathbf{B} \mathbf{y}.$$
 (36)

Using the matrix inverse lemma, we obtain

$$(\mathbf{H}^T \mathbf{H} + \mu \mathbf{I})^{-1} = \frac{1}{\mu} [\mathbf{I} - \mathbf{B}^T (\mu \mathbf{A} \mathbf{A}^T + \mathbf{B} \mathbf{B}^T)^{-1} \mathbf{B}].$$
 (37)

Using (36) and (37) in (35), line (34a) is implemented as

$$\mathbf{g} \leftarrow \frac{1}{\mu} \mathbf{B}^T (\mathbf{A} \mathbf{A}^T)^{-1} \mathbf{B} \mathbf{y} + (\mathbf{v} - \mathbf{d})$$
 (38a)

$$\mathbf{x} \leftarrow \mathbf{g} - \mathbf{B}^T (\mu \mathbf{A} \mathbf{A}^T + \mathbf{B} \mathbf{B}^T)^{-1} \mathbf{B} \mathbf{g}.$$
 (38b)

Note that the first term on the right-hand side of (38a) needs to be computed only once, because y is not updated in the loop (34); so it can be precomputed prior to the iteration.

Using (7), the solution to problem (34b) can be written as

$$\mathbf{v} \leftarrow \operatorname{soft}(\operatorname{tvd}(\mathbf{x} + \mathbf{d}, \lambda_1/\mu), \lambda_0/\mu).$$

With these simplifications, the ADMM algorithm (34) for LPF/CSD can be readily implemented. As in Section IV, all matrix operations involve only banded matrices and can therefore be implemented with high computational efficiency. The complete algorithm is listed as *Algorithm 2*.

**Algorithm 2:** For the LPF/CSD problem (32)

Input: 
$$\mathbf{y} \in \mathbb{R}^N$$
,  $\lambda_0 > 0$ ,  $\lambda_1 > 0$ ,  $\mu > 0$   
Output:  $\mathbf{x}, \mathbf{f} \in \mathbb{R}^N$   
1:  $\mathbf{v} \leftarrow \mathbf{0}$   
2:  $\mathbf{d} \leftarrow \mathbf{0}$   
3:  $\mathbf{b} \leftarrow (1/\mu) \mathbf{B}^T (\mathbf{A}\mathbf{A}^T)^{-1} \mathbf{B}\mathbf{y}$   
4: repeat  
5:  $\mathbf{g} \leftarrow \mathbf{b} + \mathbf{v} - \mathbf{d}$   
6:  $\mathbf{x} \leftarrow \mathbf{g} - \mathbf{B}^T (\mu \mathbf{A}\mathbf{A}^T + \mathbf{B}\mathbf{B}^T)^{-1} \mathbf{B}\mathbf{g}$   
7:  $\mathbf{v} \leftarrow \operatorname{soft}(\operatorname{tvd}(\mathbf{x} + \mathbf{d}, \lambda_1/\mu), \lambda_0/\mu)$   
8:  $\mathbf{d} \leftarrow \mathbf{d} - \mathbf{v} + \mathbf{x}$   
9: until convergence  
10:  $\mathbf{f} \leftarrow (\mathbf{y} - \mathbf{x}) - \mathbf{A}^{-1} \mathbf{B}(\mathbf{y} - \mathbf{x})$   
11: return  $\mathbf{x}, \mathbf{f}$ 

We note that more powerful optimization algorithms (e.g., [14], [20], [26], [28], [63]) can be used to solve not just (32) but

also extensions thereof; for example, problems that involve additional regularization terms and less friendly (i.e., non-banded) linear operators. Such algorithms are useful in dealing with more complex signal models, including constraints on signal values, and non-Gaussian noise. In this work, however, we emphasize the use of banded operators and the fused lasso signal approximator to devise an algorithm with high computational efficiency. We also strive to minimize the number of algorithm parameters beyond those appearing in the cost function (the LPF/CSD algorithm derived here has one such parameter,  $\mu$ ). Algorithms aimed for more general problems often have more such parameters.

#### VI. LTI FILTERS AND SPARSE MATRICES

This section addresses the design and implementation of discrete-time filters for the method described in Sections III–V. In particular, we describe the design and implementation of zerophase non-causal recursive high-pass filters in terms of banded matrices.

A discrete-time filter is described by the difference equation

$$\sum_{k} a(k)y(n-k) = \sum_{k} b(k)x(n-k)$$
(39)

where x(n) and y(n) are the input and output signals respectively. The frequency response of the discrete-time filter is  $H(e^{j\omega}) = B(e^{j\omega})/A(e^{j\omega})$  where B(z) and A(z) are the Z-transforms of b(k) and a(k), respectively.

We are interested in filtering finite-length signals specifically, because sparsity-based signal processing problems are generally formulated in terms of finite-length signals, and the developed algorithms are targeted for the finite-length case. In particular, this is the case for TV denoising. To implement the difference (39) for finite-length signals, we write

$$Ay = Bx$$

where  $\mathbf{A}$  and  $\mathbf{B}$  are banded matrices. The output  $\mathbf{y}$  of the filter can be written as

$$\mathbf{y} = \mathbf{A}^{-1} \mathbf{B} \mathbf{x} \tag{40}$$

which calls for the solution to a banded system. Note that for (40) to be meaningful, **B** need not be invertible, but **A** must be. Hence, **B** need not be square, but **A** must be.

Typically, there are both start- and end-transients when a discrete-time filter is applied to a finite-length signal. The start-transients depend on the initial states of the filter which, if not specified, are usually taken to be zero or optimized so as to minimize transients [50]. In the approach given here, based on  $\mathbf{y} = \mathbf{A}^{-1}\mathbf{B}\mathbf{x}$  with banded matrices, the explicit specification of initial states is avoided.

*Example:* Consider a causal first-order Butterworth high-pass filter. The difference equation has the form

$$a_0 y(n) + a_1 y(n-1) = x(n) - x(n-1)$$
(41)

which can be written and implemented as  $\mathbf{y} = \mathbf{A}^{-1}\mathbf{B}\mathbf{x}$ . The matrix  $\mathbf{B}$  is given by  $\mathbf{B} = \mathbf{D}$ , the first-order difference matrix of size  $(N-1) \times N$  defined in (2), where N is the length of the

input signal x. In this case  $\mathbf{B}_1 = \mathbf{I}_{N-1}$ . The matrix A is given by

$$\mathbf{A} = \begin{bmatrix} a_0 & & & & \\ a_1 & a_0 & & & \\ & \ddots & \ddots & & \\ & & a_1 & a_0 & \\ & & & & a_1 & a_0 \end{bmatrix}$$
(42)

and is of size  $(N-1) \times (N-1)$ .

Using  $\mathbf{y} = \mathbf{A}^{-1}\mathbf{B}\mathbf{x}$ , the filter can be applied to a length-N signal  $\mathbf{x}$ . Note that the output  $\mathbf{y}$  is of length N - 1. Due to  $\mathbf{A}$  being banded, the filter can be implemented using a fast solver for banded linear systems.

### A. Zero-Phase Filters

In order to avoid unnecessary distortion, the filter should be zero-phase; besides, expression (16) in the derivation of the problem formulation assumes the zero-phase property. The zero-phase condition is met if the frequency response  $H(e^{j\omega})$  is real-valued, or, equivalently, the temporal impulse response is symmetric.

The zero-phase property also implies specific properties of matrices  $\mathbf{A}$  and  $\mathbf{B}$ . Note that for a finite-length signal  $\mathbf{x}$ , the temporal symmetry property suggests that the filter should behave the same 'backwards' as it does 'forwards.' That is, applying the filter  $\mathbf{H}$  to the reversed version of  $\mathbf{x}$ , then reversing the filter output, should be the same as applying the filter directly to the data  $\mathbf{x}$ . Letting  $\mathbf{J}$  denote the reversal matrix (square matrix with 1's on the anti-diagonal), the filter should satisfy

$$\mathbf{JHJ} = \mathbf{H} \tag{43}$$

where the dimension of  $\mathbf{J}$  is determined by the dimensions of  $\mathbf{H}$  (recall that  $\mathbf{H}$  is rectangular). If  $\mathbf{A}$  and  $\mathbf{B}$  satisfy

$$\mathbf{J}\mathbf{A}\mathbf{J} = \mathbf{A} \quad \text{and} \quad \mathbf{J}\mathbf{B}\mathbf{J} = \mathbf{B},\tag{44}$$

then  $\mathbf{H} = \mathbf{A}^{-1}\mathbf{B}$  satisfies (43).

For the proposed LPF/TVD algorithm, the filter matrices should satisfy (44). Note that (42) does not. The following examples illustrate recursive zero-phase filters satisfying (44).

*Example:* A zero-phase non-causal second-order high-pass Butterworth filter is described by the difference equation

$$a_1y(n+1) + a_0y(n) + a_1y(n-1) = -x(n+1) + 2x(n) - x(n-1)$$
(45)

which can be defined and implemented as  $y = A^{-1}Bx$ , where B has the form

$$\mathbf{B} = \begin{bmatrix} -1 & 2 & -1 & & \\ & -1 & 2 & -1 & & \\ & & -1 & 2 & -1 & \\ & & & -1 & 2 & -1 \\ & & & & -1 & 2 & -1 \end{bmatrix}$$
(46)

and is of size  $(N - 2) \times N$ , where N is the length of the input signal **x**. For this example,  $\mathbf{B}_1 = -\mathbf{D}_{(N-2)\times(N-1)}$ .

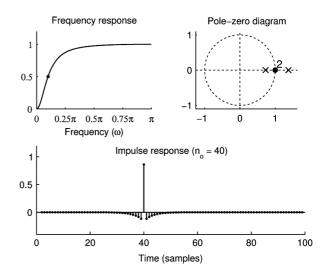


Fig. 1. Non-causal second-order high-pass filter described by (46) and (47) with cut-off frequency  $\omega_c=0.1\pi.$ 

Matrix **A** has the form

$$\mathbf{A} = \begin{bmatrix} a_0 & a_1 & & & \\ a_1 & a_0 & a_1 & & \\ & a_1 & a_0 & a_1 & \\ & & a_1 & a_0 & a_1 \\ & & & a_1 & a_0 \end{bmatrix}$$
(47)

and is of size  $(N - 2) \times (N - 2)$ . These **A** and **B** satisfy (44). Note that the output signal **y** is two samples shorter than the input signal **x**.

The transfer function of the filter (45) is given by

$$H(z) = \frac{B(z)}{A(z)} = \frac{-z + 2 - z^{-1}}{a_1 z + a_0 + a_1 z^{-1}}.$$
 (48)

In order that the filter defined by L(z) = 1 - H(z) be a low-pass filter with a zero at the Nyquist frequency (i.e.,  $\omega = \pi$ ), the gain  $c \in \mathbb{R}$  of H(z) should be unity at the Nyquist frequency. For the system (45), c is found by setting  $x(n) = (-1)^n$  and  $y(n) = c(-1)^n$  and solving for c to obtain  $c = 4/(a_0 - 2a_1)$ . Equivalently, c can be obtained as c = H(-1). Hence, for the high-pass filter (45) to have unity Nyquist gain, the coefficients should satisfy  $a_0 - 2a_1 = 4$ . Then the frequency response is given by

$$H(e^{j\omega}) = \frac{2 - 2\cos\omega}{a_0 + (a_0 - 4)\cos\omega}$$

The coefficient  $a_0$  may be set so that the frequency response has a specified cut-off frequency  $\omega_c$ . Defining  $\omega_c$  as that frequency where the frequency response is one half,  $H(e^{j\omega_c}) = 0.5$ , one obtains

$$a_0 = 4/(1 + \cos \omega_c).$$

For example, setting the cut-off frequency to  $\omega_c = 0.1\pi$ , gives  $a_0 = 2.050$ ,  $a_1 = -0.975$ . This high-pass filter is illustrated in Fig. 1. The poles are at z = 0.726 and z = 1.38 (a reciprocal pair). This recursive filter is non-causal with a 'symmetric' time-domain response (the time-domain response can not be exactly symmetric due to boundary effects in finite-length filtering).

We have referred to this recursive filter as a zero-phase filter. That usually means that the filter has a symmetric impulse response. In the context of finite-length signals, the response to an impulse  $\delta(n - n_0)$ , i.e., an impulsed located at  $n = n_0 \in \{0, \ldots, N-1\}$ , is not strictly symmetric because the response is of finite length. However, this is always the case when performing finite-length signal filtering, and it does not have a practical impact except for signals that are short relative to the decay-time of the filter.

The high-pass filter has a second-order zero at z = 1, so it annihilates constant and ramp signals, or any linear combination of these; that is, the output of the filter is identically zero whenever the input signal is of the form  $x(n) = k_0 + k_1 n$ . The preceding also is clear from inspection of the mathematical form of **B** in (46). Therefore, the low-pass filter, defined by  $\mathbf{L} = \mathbf{I} - \mathbf{H} = \mathbf{I} - \mathbf{A}^{-1}\mathbf{B}$ , exactly preserves polynomial signals of degree 1.

#### B. Higher-Order High-Pass Filter

Consider the transfer function

$$H(z) = \frac{(-z+2-z^{-1})^d}{(-z+2-z^{-1})^d + \alpha(z+2+z^{-1})^d}.$$
 (49)

The filter H(z) has a 2*d*-order zero at z = 1, so the frequency response  $H(e^{j\omega})$  is zero at  $\omega = 0$ , as are its first 2d - 1 derivatives. Also, note that H(z) can also be written as

$$H(z) = 1 - \frac{\alpha(z+2+z^{-1})^d}{(-z+2-z^{-1})^d + \alpha(z+2+z^{-1})^d}.$$

The numerator of the second term has a zero of order 2d at z = -1, so the frequency response  $H(e^{j\omega})$  has unity gain at  $\omega = \pi$ , and its first 2d - 1 derivatives are zero there. That is, the frequency response is maximally-flat at  $\omega = 0$  and at the Nyquist frequency; hence, this is a zero-phase digital Butterworth filter.

The filter H(z) in (49) is defined by the positive integer dand by  $\alpha$ . The parameter  $\alpha$  can be set so that the frequency response has a specified cut-off frequency  $\omega_c$ . Setting the gain at the cut-off frequency to one half,  $H(e^{j\omega_c}) = 0.5$ , gives the equation

$$\frac{(1-\cos\omega_c)^d}{(1-\cos\omega_c)^d+\alpha(1+\cos\omega_c)^d}=\frac{1}{2}.$$

Solving for  $\alpha$  gives

$$\alpha = \left(\frac{1 - \cos \omega_c}{1 + \cos \omega_c}\right)^d.$$

The zero-phase high-pass Butterworth filter (49) can be implemented as  $y = A^{-1}Bx$  where

- 1) **B** is a banded matrix of size  $(N 2d) \times N$ .
- 2) A is a square symmetric banded matrix of size  $(N 2d) \times (N 2d)$ .
- 3) Both A and B have bandwidth 2d+1; that is, in addition to the main diagonal, they have d diagonals above and below the main diagonal.

Note that this filter maps an input signal of length N to an output signal of length N - 2d. When d = 1, we get the high-

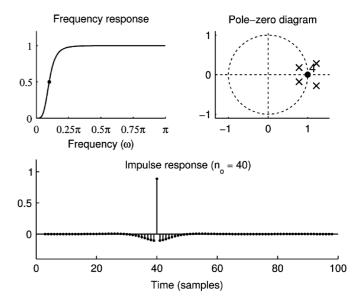


Fig. 2. Non-causal fourth-order high-pass filter (49) with cut-off frequency  $\omega_c=0.1\pi$  and d=2.

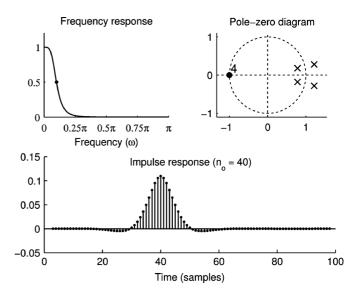


Fig. 3. Non-causal fourth-order low-pass filter (50) with cut-off frequency  $\omega_c = 0.1\pi$  and d = 2.

pass filter (48) as a special case. In this case, A and B, given by (46) and (47), are tridiagonal (a bandwidth of 3).

*Example:* Set d = 2 and the cut-off frequency to  $\omega_c = 0.1\pi$ . The matrix **B** is of size  $(N - 4) \times N$  and has the form

$$\mathbf{B} = \begin{bmatrix} 1 & -4 & 6 & -4 & 1 & & \\ & 1 & -4 & 6 & -4 & 1 & \\ & & \ddots & & & \ddots & \\ & & & 1 & -4 & 6 & -4 & 1 \end{bmatrix}$$

with bandwidth 5. For this example, **B**<sub>1</sub> has non-zero elements [-1, 3, -3, 1] in each row. With  $\omega_c = 0.1\pi$ , one obtains  $\alpha = 6.29 \times 10^{-4}$ . **A** will be a banded symmetric square matrix with bandwidth 5. The coefficients of **A** are  $a_0 = 6.0038$ ,  $a_1 = -3.9975$ ,  $a_2 = 1.0006$ , where  $a_i$  lies on diagonal  $\pm i$ . The resulting fourth-order zero-phase filter is shown in Fig. 2.

# C. Low-Pass Filter

The LPF/TVD algorithm provides an estimate,  $\hat{x}$ , of the sparse-derivative component and calls for the high-pass filter  $\mathbf{H} = \mathbf{A}^{-1}\mathbf{B}$ . The algorithm does not use a low-pass filter. But, to obtain an estimate  $\hat{f}$  of the low-pass component, recall that we need the low-pass filter denoted above as LPF = I - HPF. A low-pass filter of this form is trivially performed by subtracting the high-pass filter output from its input. However, note that for the high-pass filter described in Section VI-B, the matrices **B** and **H** are rectangular. Consequently, the output of the high-pass filter is shorter than its input by 2dsamples (d at the beginning and d at the end). Hence, to implement the low-pass filter, the input signal should likewise be truncated so that the subtraction involves vectors of equal length. Consequently, the low-pass filter can be expressed as  $LPF(\mathbf{x}) = TRUNC(\mathbf{x}) - HPF(\mathbf{x})$  where  $TRUNC(\mathbf{x})$  denotes the symmetric truncation of  $\mathbf{x}$  by 2d samples.

The low-pass filter matrix,  $\mathbf{L}$ , is therefore given by  $\mathbf{L} = \mathbf{\bar{I}}_d - \mathbf{A}^{-1}\mathbf{B}$  where  $\mathbf{\bar{I}}_d$  is the identity matrix with the first d and last d rows removed. The matrix  $\mathbf{\bar{I}}_d$  is of size  $(N - 2d) \times N$ . The signal  $\mathbf{\bar{I}}_d \mathbf{x}$  is obtained by deleting the first d and last d samples from  $\mathbf{x}$ .

Based on the high-pass filter (49), the low-pass filter L(z) := 1 - H(z) has the transfer function

$$L(z) = \frac{\alpha(z+2+z^{-1})^d}{(-z+2-z^{-1})^d + \alpha(z+2+z^{-1})^d}$$
(50)

with a 2*d*-order zero at z = -1. The filter matrix is given by  $\mathbf{L} = \bar{\mathbf{I}}_d - \mathbf{A}^{-1} \mathbf{B}$ .

*Example:* From the high-pass filter shown in Fig. 2 with d = 2, we obtain the low-pass filter illustrated in Fig. 3. The filter can be implemented as  $\mathbf{y} = \mathbf{\bar{I}}_2 \mathbf{x} - \mathbf{A}^{-1} \mathbf{B} \mathbf{x}$ . This filter passes third-order signals (of the form  $x(n) = k_0 + k_1 n + k_2 n^2 + k_3 n^3$ ) with no change, except for truncation by two samples at start and end.

## VII. EXAMPLES

The following examples illustrate the use of the algorithms derived in Sections IV and V for the LPF/TVD and LPF/CSD problems, respectively.

## A. LPF/TVD Example 1

To illustrate simultaneous low-pass filtering and total-variation denoising, we apply Algorithm 1 (Section IV) to the noisy data y shown in Fig. 4. This is the same data used in the first example of [71], where smoothing was performed using a (non-time-invariant) least-squares polynomial approximation. The signal consists of a low-frequency sinusoid, two additive step discontinuities, and additive white Gaussian noise. In order to apply the new algorithm, we must specify a high-pass filter **H** and regularization parameter  $\lambda$ . We use the fourth-order filter (49) with d = 2 and cut-off frequency  $\omega_c = 0.044\pi$ . The parameter  $\lambda$  was set to 0.8 based on (31). The algorithm was run for 30 iterations.

Fig. 4 shows the sparse-derivative component  $\mathbf{x}$  obtained from the algorithm. The low-pass component  $\mathbf{f}$  is obtained by low-pass filtering  $\mathbf{y} - \mathbf{x}$ ; it is given by  $\mathbf{f} = \mathbf{L}(\mathbf{y} - \mathbf{x}) = \overline{\mathbf{I}}_2(\mathbf{y} - \mathbf{x}) - \mathbf{H}(\mathbf{y} - \mathbf{x})$ . The total LPF/TVD output,  $\mathbf{f} + \mathbf{x}$ , shown in the fourth panel of Fig. 4, substantially

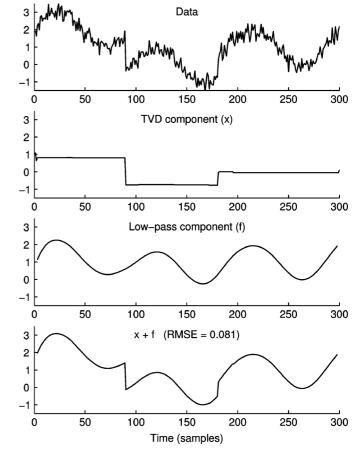


Fig. 4. LPF/TVD Example 1. Simultaneous low-pass filtering and total variation denoising. From the noisy data, the sparse-derivative and low-pass components are obtained individually. Algorithm parameters: d = 2,  $\omega_c = 0.044\pi$ ,  $\lambda = 0.8$ .

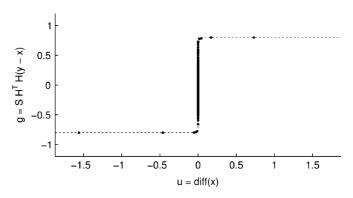


Fig. 5. LPF/TVD Example 1. The scatter plot verifies that optimality condition (30) is satisfied.

smooths the data while preserving the discontinuities, without introducing Gibbs-like phenomena.

The optimality condition (30) is illustrated in Fig. 5 as a scatter plot. Each point represents a pair (g(n), u(n)), where g(n) and u(n) denote the *n*-th time samples of signals g and u. Note that (30) means that if each pair (u, g) lies on the graph of the step function indicated as a dashed line in Fig. 5, then the computed x does minimize the objective function in (19). It is seen that most of the points lie on the line u = 0, which reflects the sparsity of **D**x.

As noted in the Introduction, the earlier work in [71] (specifically, the LoPATV algorithm) can also be used to perform the type of processing achieved by the new algorithm. Accordingly, the result shown in Fig. 4 is comparable to the result in [71], which compared favorably to several other methods, as shown therein. However, while the method of [71] calls for the polynomial degree, block length, and overlapping-factor to be specified, the new method calls for the low-pass filter characteristics to be specified (filter order and cut-off frequency). The latter parameters have the benefit of being more in line with conventional filtering practice and notions.

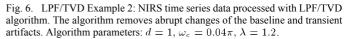
To further contrast the new algorithm with LoPATV, we note that the LoPATV algorithms requires that two parameters ( $\mu_0$ and  $\mu_1$ ) be specified, which raises the issue of how to set these values in order to obtain fast convergence. In contrast, Algorithm 1 formulated in this work does not involve any parameters beyond those in the problem statement (19), and is computationally fast. Thirty iterations of Algorithm 1 takes about 13 milliseconds on a 2013 MacBook Pro (2.5 GHz Intel Core i5) running Matlab R2011a. Run-times reported in subsequent examples are obtained using the same computer.

## B. LPF/TVD Example 2

Fig. 6 illustrates the use of Algorithm 1 on 304 seconds of NIRS time series data. The data has a sampling rate of 6.25 samples/second (length N = 1900). The data used for this example is the record of the time-dependent NIRS light-intensity level, for one channel in a multi-probe physiological measurement session. All of the light-emitting and -receiving optodes, where an optode is the optical analogue of an EEG electrode, were located on the scalp of an adult male research-study subject. The terms 'source' and 'detector' are used to refer to a light-emitting optode and a light-receiving optode, respectively, and a measurement channel is defined by specifying a particular source-detector pair. For example, for the channel considered here, the source and detector were located on the subject's scalp over the back of the head. NIRS data from measurements of this type are susceptible to subject-motion artifacts, as indicated in Section I-B. In some cases, and as seen most strikingly at approximately the 80-second mark, motion can cause a change in optode-skin contact sufficient to produce an abrupt, permanent shift in the baseline value. It can be observed that the TVD component produced by the algorithm successfully captures the discontinuities and transient artifacts present in the data. The LPF/TVD algorithm was run for 30 iterations with a total run time of 30 milliseconds.

To concretely illustrate the benefits of LPF/TVD in comparison with LTI filtering alone, we consider the problem of detrending (baseline removal). When a zero-phase LTI highpass filter is used to remove the baseline of the data shown in Fig. 6, we obtain the detrended signal illustrated in Fig. 7. The abrupt jumps in the data produce transients in the detrended data—an unavoidable consequence of LTI filtering. However, if the TV component obtained using LPF/TVD is subtracted from the data prior to LTI high-pass filtering, then the transients are greatly reduced, as illustrated in the figure. The near-elimination of the transients is possible because the LPF/TVD algorithm is nonlinear.

A further benefit of LPF/TVD processing is revealed in the frequency domain. In particular, the Welch periodogram in Fig. 7 shows that LPF/TVD preprocessing reduces the strong,



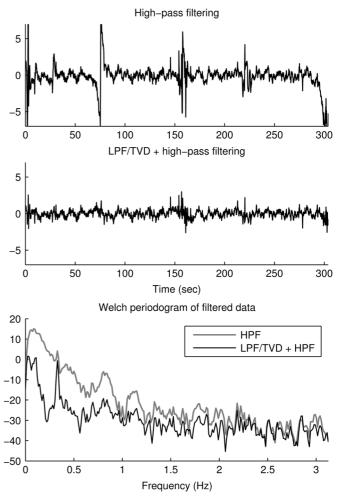
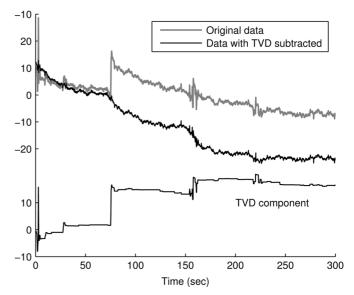


Fig. 7. LPF/TVD Example 2. Detrending by high-pass filtering and by LPF/TVD prior to high-pass filtering. In the periodogram, LPF/TVD uncovers a signal component at frequency 0.32 Hz which is otherwise obscured by the broad low-frequency energy due to strong transients.

broad low-frequency energy due to the transients. Consequently, a signal component at about 0.32 Hz, which in the HPF



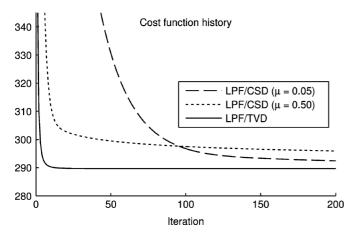


Fig. 8. LPF/CSD Example 1. Comparison of convergence of Algorithm 1 (LPF/TVD) and Algorithm 2 (LPF/CSD).

result is obscured by the broad power spectrum arising from the transients, is unambiguously revealed. Notably, this lies within the range of typical human respiration frequencies (12–20 cycles/min). The respiratory rhythm is frequently observed in data from NIRS physiological measurements [3], [8], and PSD analysis of relatively artifact-free channels from the same recording session indicate that the participant's respiratory frequency was indeed about 0.32 Hz. This example shows how the LPF/TVD method can be used to improve the effectiveness of LTI filtering and spectral analysis.

#### C. LPF/CSD Example 1

Note that the LPF/CSD problem (32) generalizes the LPF/TVD problem (19). Specifically, the LPF/TVD problem is recovered with  $\lambda_0 = 0$  in (32). Hence, Algorithm 2 (Section V) can be used to solve the LPF/TVD problem. For example, it can be used to perform the processing illustrated in Fig. 6 for which we used Algorithm 1. Consequently, it may appear that Algorithm 1 is unnecessary. However, in the following, we demonstrate two advantages of Algorithm 1, in comparison with Algorithm 2, for solving the LPF/TVD problem.

In order to compare the convergence behavior of Algorithms 1 and 2, we apply both of them to the data shown in Fig. 6 ("Original data" in gray). The Algorithm 2 result is visually indistinguishable from that obtained with Algorithm 1, so we do not illustrate it separately.

The cost function history of each algorithm is illustrated in Fig. 8. Algorithm 1 converges well within 30 iterations. Note, however, that Algorithm 2 requires the user to specify a parameter  $\mu > 0$ , which can be interpreted as a type of step-size parameter. As illustrated in Fig. 8, the convergence behavior of Algorithm 2 depends on  $\mu$ . For  $\mu = 0.5$ , the algorithm initially converges quickly but has very slow long-term convergence. For  $\mu = 0.05$ , the algorithm has better long-term convergence, but poor initial convergence. Note that Algorithm 1 converges much faster than Algorithm 2, regardless of  $\mu$ .

In comparison with Algorithm 2, Algorithm 1 has two advantages. First, it does not require the user to specify a parameter  $\mu$ . Second, it often converges faster regardless of what value of  $\mu$ is used for Algorithm 2. On the other hand, Algorithm 2 solves the more general problem of LPF/CSD and can therefore perform processing that is not possible with Algorithm 1.

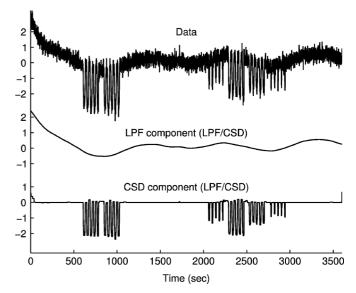


Fig. 9. LPF/CSD Example 2. Near infrared spectroscopic (NIRS) data and LPF/CSD processing. The method simultaneously performs low-pass filtering and sparse signal denoising.

We remark that the LoPATV algorithm [71] (which performs LPF/TVD-type processing) requires the specification of two parameters. Hence, it is even more affected by the issues of (1) parameter tuning for fast convergence and (2) fastest achievable convergence.

## D. LPF/CSD Example 2

To illustrate simultaneous low-pass filtering and compound sparse denoising (LPF/CSD), we have obtained data from a dynamic tissue-simulating phantom [9], while varying the strength of its absorption for NIR light in a manner that emulates the hemodynamic response of a human brain to intermittently delivered stimuli. Fig. 9 illustrates data acquired by the system. The signal is of length 4502 samples, with a sampling rate of 1.25 samples/second and an observation time of 3602 seconds. The 'hemodynamic' pulses are observed in the presence of unavoidable low-frequency background processes and wideband noise. The signal of interest and its derivative are sparse relative to the low-frequency background signal and noise. For the illustrated measurement channel, the noise standard deviation is greater than 10% of the largest-magnitude hemodynamic pulse; this is not an uncommon noise level for physiological NIRS data [3]. Algorithm 2 simultaneously estimates and separates the low-pass background signal and the hemodynamic pulses, as illustrated in Fig. 9. For this computation, 50 iterations of the algorithm were performed, in a time of 70 milliseconds. The pulses are illustrated in detail in Fig. 10. Note that the shapes of the pulses are well preserved, in contrast to the commonly observed amplitude-reducing, edge-spreading, and plateau-rounding, of LTI filtering alone (see Fig. 10(b)).

For comparison, Fig. 10 illustrates the output of a band-pass filter (BPF) applied to the same noisy data. Note that the BPF signal exhibits both more baseline drift and more noise than the CSD component produced by LPF/CSD processing. In particular, the BPF obscures the amplitude of the hemodynamic pulses relative to the baseline. While the band-edges of the BPF can be adjusted to obtain a different BPF signal from the one

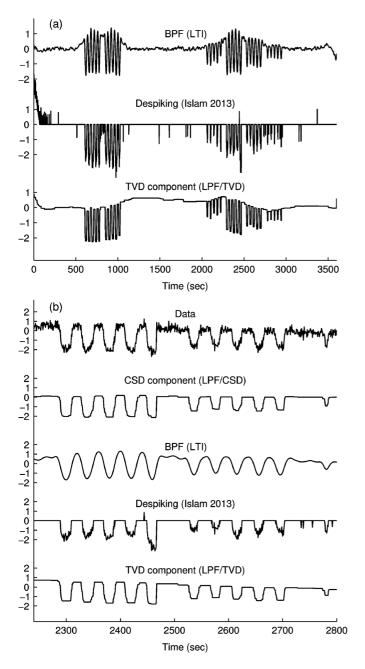


Fig. 10. LPF/CSD Example 2. For the data in Fig. 9, the output of a bandpass filter (BPF), a de-spiking algorithm [54], and the TVD component obtained using LPF/TVD are shown for comparison with LPF/CSD. (a) Full duration of the data time series. (b) Expanded view of a brief portion of the time series.

shown here, these adjustments will either increase the residual noise level, increase the baseline drift, or further distort the shape of the hemodynamic pulses.

For further comparison, Fig. 10 also illustrates the output of a recent de-spiking algorithm [54]; see also [48]. The algorithm is based on clustering in phase-space, wherein the state vector consists of both the value of the signal and its derivative. This de-spiking algorithm simultaneously uses both the signal value and its derivative, like the LPF/CSD approach derived here. However, it does not explicitly account for the presence of a low-pass component. It can be observed that some false peaks occur and that residual noise remains on the crests of the peaks. The result was obtained using software by the author at http://www.mathworks.com/matlabcentral/fileexchange/.

Finally, the result of LPF/TVD processing is also shown in Fig. 10. It can be seen that the TVD component produced by Algorithm 1 is similar to the CSD component produced by Algorithm 2; however, it exhibits baseline drift. Algorithm 1 cannot achieve a baseline value of zero due to the absence in (19) of the  $\lambda_0$  term that is present in (32).

## E. LPF/CSD Example 3

The LPF/CSD approach can also be used for artifact reduction, as illustrated in Fig. 11. The data is a 300-second NIRS time series from the same experimental measurement as in LPF/TVD Example 2 above. However, for the channel considered here, the source and detector were located on the subject's forehead in the vicinity of his left eye. This makes the data susceptible to motion artifacts due to eve blinks (in addition to all other sources of motion artifact that ordinarily are present). The data is corrupted by transients of variable amplitude, width, and shape. The CSD component was obtained using 50 iterations of Algorithm 2 with a total run-time of 30 milliseconds. Fig. 11 displays a 100-second interval of the 300-second signal, to more clearly show the details of the data. The CSD component captures the transients with reasonable accuracy while maintaining a baseline of zero. Subtraction of the CSD component from the original data demonstrates that the algorithm has largely removed the artifacts while leaving the (physiological) oscillatory behavior intact.

The benefit can also be seen in the frequency domain. When the CSD component is subtracted from the data, the periodogram shows a broad peak in the 1.0–1.2 Hz band. Notably, this lies within the range of typical human cardiac (i.e., heartbeat) frequencies (60–100 cycles/min). The cardiac rhythm is frequently observed in data from NIRS physiological measurements [3], [8], and PSD analysis of relatively artifact-free channels from the same recording session indicate that the participant's cardiac frequency was indeed approximately 1.1 Hz. In the periodogram of the original data, this peak is obscured by the broad-band energy of the transient artifacts.

For comparison, Fig. 12 illustrates the output of two recent algorithms, the de-spiking algorithm of [54] and the motion artifact reduction algorithms of [36]. This second method, which was implemented using the NAP software application written by the authors of [36], [37], identifies outliers in a high-pass filtered version of the time series, based on a user-specified z-score threshold. These values are then replaced: a simple linear interpolation is used for 'spikes' (i.e., artifacts briefer than a user-specified maximum duration); for 'ripples' (i.e., artifacts for which the number of consecutive data values having supra-threshold z-scores exceeds a user-specified minimum), the data are approximated with piecewise-continuous cubic polynomials, and the corrected data are the differences between the original data and the best-fitting cubics. Elsewhere in the time series, the original data are not modified.

It can be observed in Fig. 12 that the algorithms of [36], [54] successfully identify high-amplitude spikes, but yield restored time-series that are less regular than the proposed method.

Both methods [36], [54] are based on a two-step procedure: first identify spikes (or ripples); second, interpolate to fill in the



Example	Run-time	Signal length	Iterations
LPF/TVD 1	13 ms	300	30
LPF/TVD 2	30 ms	1900	30
LPF/CSD 2	70 ms	4502	50
LPF/CSD 3	30 ms	1900	50

and non-artifact data points, and is flexible in terms of the types of artifacts it can handle.

# F. Run-Times

The run-times from the examples of Algorithm 1 and Algorithm 2 for LPF/TVD and LPF/CSD respectively, are summarized in Table I.

#### VIII. CONCLUSION

Sparsity-based signal processing methods are now highly developed, but in practice LTI filtering still is predominant for noise reduction for 1-D signals. This paper presents a convex optimization approach for combining low-pass filtering and sparsity-based denoising to more effectively filter (denoise) a wider class of signals. The first algorithm, solving the LPF/TVD problem (19), assumes that the signal of interest is composed of a low-frequency component and a sparse-derivative component. The second algorithm, solving the LPF/CSD problem (32), assumes the second component is both sparse and has a sparse derivative. Both algorithms draw on the computational efficiency of fast solvers for banded linear systems, available for example as part of LAPACK [4].

The problem formulation and algorithms described in this paper can be extended in several ways. As in [71], enhanced sparsity can be achieved by replacing the  $\ell_1$  norm by regularizers that promote sparsity more strongly, such as the  $\ell_p$  pseudonorm  $(0 , or by reweighted <math>\ell_1$  [18], greedy  $\ell_1$  [58], etc. In addition, in place of total variation, higher-order or generalized total variation can be used [56]. The use of LTI filters other than a low-pass filter may also be useful; for example, the use of band-pass or notch filters may be appropriate for specific signals. It is envisioned that more general forms of the approach taken in this paper will demand more powerful optimization algorithms than those employed here. In particular, recently developed optimization frameworks based on proximity operators [14], [20], [26], [28], [63], [66] are specifically geared to problems involving sums of non-smooth convex functions (i.e., compound regularization).

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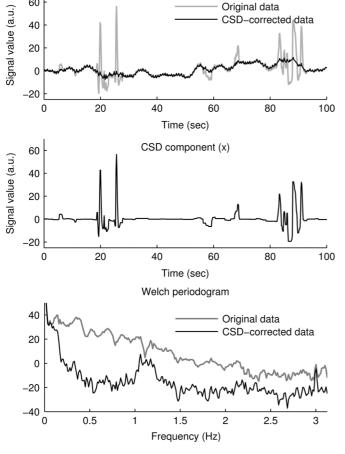


Fig. 11. LPF/CSD Example 3. Removal of artifacts from a NIRS time series by LPF/CSD processing.

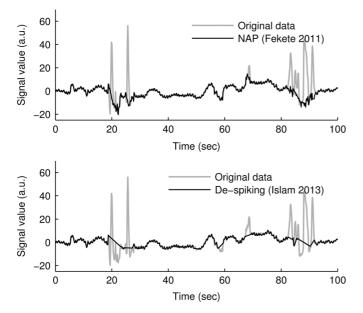


Fig. 12. LPF/CSD Example 3. Result of NAP [36] and de-spiking [54].

gaps. In addition, neither method attempts to identify or correct additive steps in the data, and hence they are not effective for examples where LPF/TVD can be used. In contrast, the proposed method consists of a single problem formulation, which does not rely on a segmentation of the time series into artifact

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**Ivan W. Selesnick** (S'91–M'98–SM'08) received the B.S., M.E.E., and Ph.D. degrees in electrical engineering in 1990, 1991, and 1996 from Rice University, Houston, TX. In 1997, he was a visiting professor at the University of Erlangen-Nurnberg, Germany. He then joined the Department of Electrical and Computer Engineering, NYU Polytechnic School of Engineering, New York (then Polytechnic University), where he is associate Professor.

His current research interests are in the area of digital signal and image processing, wavelet-based

signal processing, sparsity techniques, and biomedical signal processing. He has been an associate editor for the IEEE TRANSACTIONS ON IMAGE PROCESSING, IEEE SIGNAL PROCESSING LETTERS, and IEEE TRANSACTIONS ON SIGNAL PROCESSING.



Harry L. Graber (M'95) received the A.B. degree in chemistry from the Washington University, St. Louis, MO, in 1983, and the Ph.D. degree in physiology and biophysics from SUNY Downstate Medical Center, Brooklyn, NY, in 1998.

He subsequently became a Research Associate (1998) and then a Research Assistant Professor (2001) at SUNY Downstate Medical Center. Since 2001 he also has been the Senior Applications Specialist for NIRx Medical Technologies. His research interests include diffuse optical imaging algorithms,

and application of feature extraction and time-series analysis methods for interpretation of biological signals.





**Douglas S. Pfeil** received the B.S. degree in biochemistry from Lehigh University, Bethlehem, PA, in 2007. He is an M.D./Ph.D. candidate in the Molecular and Cellular Biology Program at SUNY Downstate Medical Center, Brooklyn, NY.

His research interests include near infrared imaging of the human and primate brain, particularly changes that can occur during surgery. Previously, he studied the molecular biology of nerve cell growth cones in the Wadsworth laboratory at Robert Wood Johnson University Hospital.

**Randall L. Barbour** received the Ph.D. degree in biochemistry from Syracuse University, Syracuse, NY, in 1981. This was followed by a postdoctoral fellowship in Laboratory Medicine at SUNY at Buffalo.

He is currently Professor of Pathology at SUNY Downstate Medical Center, and Research Professor of Electrical Engineering at Polytechnic University, Brooklyn, NY. He is an originator of the field of diffuse optical tomography and is co-founder of NIRx Medical Technologies, LLC. He has an extensive

background in a broad range of medical and scientific and technical fields.