



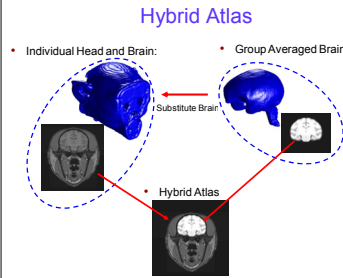
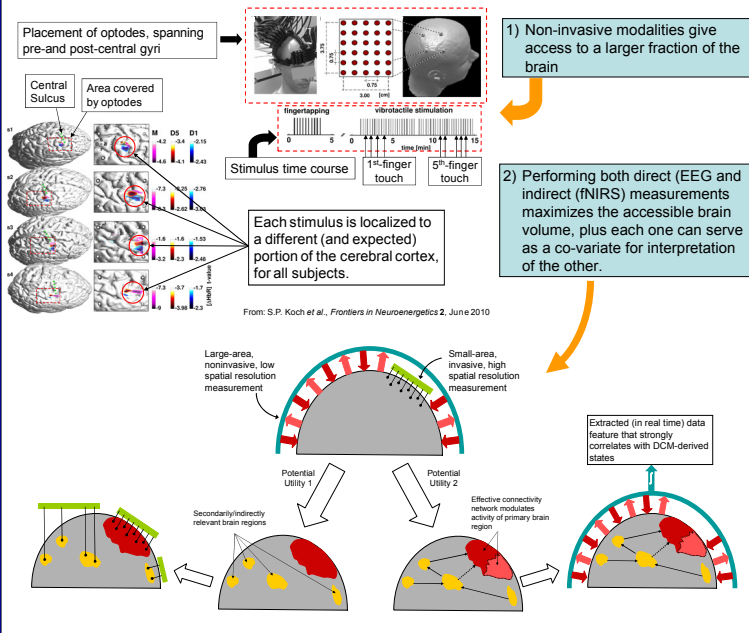
Development of Whole-Brain Activity Measures to Aid in Optimization of BCI Performance

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B.M.I. – implant interprets neuroactivity signals;
decides what action the person/animal wishes to perform; actuates it



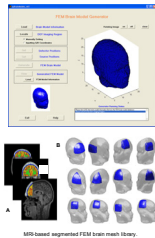
Prior (Human Head) Anatomical Mapping Work

1. 3D FEM brain model generator:
Supports easy specification of user-defined image operators for a selected sensing array configuration.

a. MR-based FEM model library:

- Establish segmented FEM brain atlas from MRI of selected subjects).
- Divide brain into 25 overlapping regions, each comprising 3000-3600 nodes, with each region having a surface area of 50-75 cm² and a maximum depth of up to 5 cm.
- Compute solutions to forward diffusion problem, using Type III boundary conditions, for each of nearly 400 outer surface nodes per region.
- Compute joint intensity probabilities for all possible source-detector combinations, to generate associated Jacobian matrix (~160,000 pairs/ROI).

b. User interface

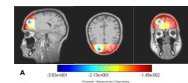


Software Validation

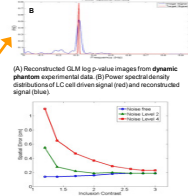
2. Software validation:

a. Sensitivity to Expected Experimental Uncertainty:

Findings demonstrate that mapping errors vary from 3-10 mm with the largest error occurring at edge of S/D region.



b. Phantom Study: Introduce Hb signal at known location and dynamics.



4) Detailed anatomical picture of subject's head improves solution accuracy and spatial resolution

- a) Imaging operators take the details of the inhomogeneous, irregularly shaped, medium into account
- b) A single, standard head, that data from individual subjects is projected onto, minimizing effects of individual variation
- c) All of the advantages gained from using normalized difference strategies apply

5) Well-characterized methods for analyzing time series (e.g., GLM) can be used to accurately identify which brain regions consistently participate in planning ("thinking about") and performing the task under study

Functional connectivity

- Seed-voxel correlation analyses (e.g., GLM)
- Eigenimage analysis
 - Principal Component Analysis (PCA)
 - Singular Value Decomposition (SVD)
 - Partial Least Squares (PLS)
- Independent Component Analysis (ICA)

Pros:
◊ useful when we have no model of what caused the data (e.g., sleep, hallucinations)
Cons:
◊ no mechanistic insight into the neural system of interest
◊ inappropriate for situations where we have a priori knowledge and experimental control over the system of interest

Effective connectivity

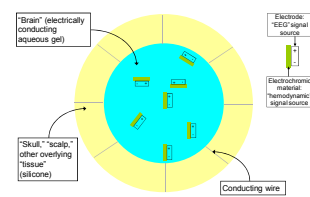
- Structural Equation Modelling (SEM)
- Psycho-physiological interactions (PPI)
- Multivariate autoregressive models (MAR)
- Granger causality techniques
- Kalman filtering
- Volterra series
- Dynamic Causal Modelling (DCM)

Pros:
◊ useful when we have a model of what caused the data
Cons:
◊ inappropriate if cerebral dynamics do not closely approximate theoretical assumptions underlying the method

DCM: Distinguished from others:
◊ accommodating the nonlinear and dynamic aspects of neuronal interactions
◊ framing the estimation problem in terms of perturbations that accommodate experimentally designed inputs

3) While GLM integrates over time, techniques such as DCM can be used to derive a high level of information – effective connectivity – from detailed differences between the timings of responses in different regions.
a) Premium on SNR and undistorted imaging data (recovered value proportional to what is actually present)

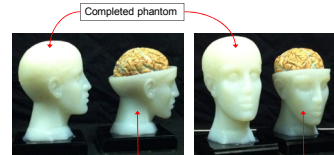
fNIRS/EEG Dynamic Phantom: concept



6) Dynamic phantom – provides unequivocal mechanism for assessing the accuracy of an effective connectivity algorithm (e.g., DCM)

- a) Always know what The Right Answer is, because that's input
- b) Both the modulatory effects among brain regions, and the magnitude and timing of the hemodynamic response function, can be experimentally controlled

fNIRS/EEG Dynamic Phantom: example



c) Testbed for assessing the impact of including/leaving out regions (e.g., ones identified from the noninvasive measurement) on the performance of the effective connectivity computations

Acknowledgements

This work was supported by the Defense Advanced Research Projects Agency, and by the NIH under grants no. R42NS050007 and no. R44NS049734 to R.L. Barbour, and by EU grants NEST 012778, EFRE 2002000009, and nEURoCpt 201076.

Central idea:
Brain ↔ Deterministic nonlinear dynamic system
Effective connectivity is parameterized in terms of coupling among unobserved brain states (e.g., neuronal activity in different regions)
Objective:
To estimate the parameters by perturbing the system and measuring the response

Neuronal states: $z(t) = \begin{bmatrix} z_1(t) \\ \vdots \\ z_n(t) \end{bmatrix}$

State equations: $\dot{z} = \frac{dz}{dt} = \begin{bmatrix} f_1(z_1, \dots, z_n, u, \theta_1) \\ \vdots \\ f_n(z_1, \dots, z_n, u, \theta_n) \end{bmatrix}$

in general: $\dot{z} = F(z, u, \theta)$

u : external input
 $\theta = \{\theta_1, \dots, \theta_n\}$: system parameters, specify the nature of the interactions

Visual Stimulus Paradigm

motion attention? H1 H2

Alternative hypotheses regarding which pathway the input modulates (i.e., which elements of matrix B are non-zero)

	Motion Effect, Attention Effect	Volume Doubled	Sphere → Cube, Volume Preserved	Center Moved by 1/2 Radius	Original Radius Doubled
H 1:	0.409, 0.176	0.386, 0.162	0.384, 0.167	0.321, 0.121	0.321, 0.147
H 2:	0.400, 0.345	0.381, 0.329	0.378, 0.337	0.327, 0.293	0.319, 0.334

Stability Analysis. Note that interpretation of DCM parameters is based on trends (e.g., motion effect > attention effect), not on the exact numerical values.

The relative magnitudes of the computed parameters has flipped (motion effect < attention effect)